NASA/TM-2004-212982



Printed Multi-Turn Loop Antenna for RF Bio-Telemetry

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Prepared for the 2004 Antennas and Propagation Society International Symposium and URSI National Radio Science Meeting sponsored by the Institute of Electrical and Electronics Engineers Monterey, California, June 20–26, 2004

National Aeronautics and Space Administration

Glenn Research Center

Acknowledgments

The NASA Glenn Research Center's Technology Trans	fer and Partnership Office supported this work under the
research project entitled "RF Telemetr	y for Bio-MEMS Sensors and Actuators".

This report contains preliminary findings, subject to revision as analysis proceeds.

Available from

NASA Center for Aerospace Information 7121 Standard Drive Hanover, MD 21076 National Technical Information Service 5285 Port Royal Road Springfield, VA 22100

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Abstract—In this paper, a novel printed multi-turn loop antenna for contact-less powering and RF telemetry from implantable bio-MEMS sensors at a design frequency of 300 MHz is demonstrated. In addition, computed values of input reactance, radiation resistance, skin effect resistance, and radiation efficiency for the printed multi-turn loop antenna are presented. The computed input reactance is compared with the measured values and shown to be in fair agreement. The computed radiation efficiency at the design frequency is about 24 percent.

I. INTRODUCTION

The biological and physical sciences program at NASA seeks to develop telemetry based implantable sensing systems to monitor the physiological parameters of humans during space flights [1]. This focus is rather unique when compared to efforts by other investigators, which have been mainly in the area of RF/microwave applications in medical treatment and biological effects [2].

In this paper, we present the development of a printed multi-turn loop antenna for contact-less powering and RF telemetry to acquire data from implantable bio-microelectromechanical systems (bio-MEMS) based capacitive pressure sensors. This effort is part of a U.S. patent that has been recently granted [3]. Several researchers in the past [4–6] have demonstrated RF antennas for telemetry reception from implantable sensors, and table I summarizes the type and dimensions of these antennas. However, the unique aspects of our approach are as follows: first, we make use of a multi-turn loop antenna printed on a dielectric substrate with a central annular region. The central annular region facilitates housing of signal processing circuits and thus lowers the height profile of the packaged hand-held unit. Second, the diameter of our loop antenna is significantly smaller which makes the hand-held unit very compact.

II. RF TELEMETRY SYSTEM

The contact-less powering and telemetry concept, is illustrated in figure 1(a). To obtain a pressure reading, a pulse emitted by the external hand-held unit initially interrogates the implanted sensor. The pulse induces a voltage in the implanted sensor inductor thus implementing contact-less powering. The waveform of this induced voltage is a decaying sine wave. Since the inductance is fixed, the frequency of the decaying sine wave is mainly determined by the capacitance of the pressure sensor. The energy radiated by the inductor during these oscillations is picked up as a telemetry signal by the receiving antenna in the hand-held unit. The notional wireless RF telemetry system [3] is illustrated in figure 1(b).

Table I: The diameter and the type of antenna used in RF biotelemetry systems

Type of antenna	Antenna diameter, mm	Reference
Planar spiral	80	Von Arx and Najafi [4]
Disk coils	90	Hamici, Itti, and
		Champier [5]
Solenoid coils	100 to 150	Troyk and Edgington [6]
Printed multi-turn loop	51	This paper

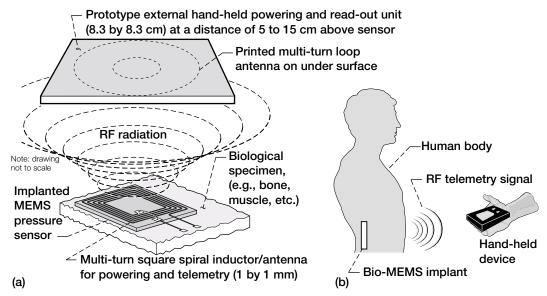


Figure 1.—Contact-less powering and telemetry. (a) Concept. (b) Application in biosensors.

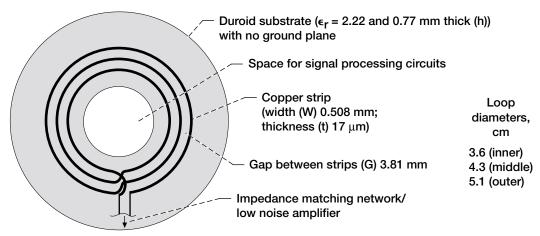


Figure 2.—Printed multi-turn loop antenna on a dielectric ring.

III. MULTI-TURN LOOP ANTENNA ON A DIELECTRIC RING

A. Input Reactance, Radiation Resistance, and Skin Effect Resistance

The multi-turn loop antenna is illustrated in figure 2. The presence of a dielectric substrate of relative dielectric constant ε_r is taken into consideration in the computer model by assuming that the loop is embedded in a medium of effective dielectric constant equal to $(\varepsilon_r + 1)/2$, [7]. In addition, the loop strip conductor of width W and thickness t is replaced by an equivalent wire of diameter d = 0.25 W [8]. Under these assumptions, the multi-turn loop with total perimeter P is modeled as an equivalent lossless shorted transmission line of length l = P/2 [9]. The input reactance of the loop is then equal to the transmission line input reactance. The skin effect resistance and the radiation resistance of the loop are determined using equations in [7] and [10], respectively.

IV. COMPUTED/MEASURED RESULTS AND DISCUSSIONS

The computed and measured reactive part of the input impedance ($Z_{\rm in}$) is shown in figures 3(a) and 3(b), respectively. To measure the $Z_{\rm in}$ of the antenna in figure 2, a short length of a coax is soldered to the circuit and the data acquired using a microwave network analyzer (Model HP 8510C). The computed and measured results are in fair agreement. The discrepancy is because of the phase introduced by the short length of coax that is needed for interface with the test instruments, which is not trivial to calibrate out. The computed skin effect and the radiation resistances are presented in figures 4 and 5, respectively. From these results the radiation efficiency is calculated and shown in figure 6. The radiation efficiency at the design frequency of 300 MHz is about 24 percent.

V. CONCLUSIONS

The paper demonstrates a novel printed multi-turn loop antenna for contact-less powering and RF telemetry from implantable bio-MEMS sensors at 300 MHz. In addition, computed values of input reactance, radiation resistance, skin effect resistance, and radiation efficiency for the loop antenna are presented. The computed input reactance is compared with the measured values and shown to be in fair agreement. The computed radiation efficiency of the loop antenna at 300 MHz is about 24 percent.

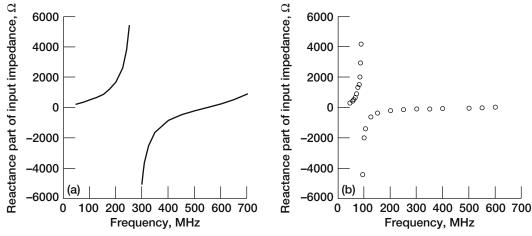


Figure 3.—Input reactance. (a) Computed. (b) Measured.

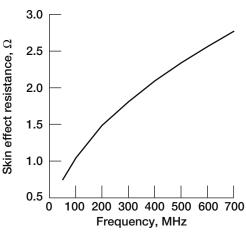


Figure 4.—Computed skin effect resistance.

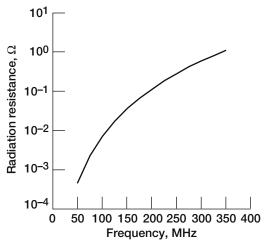


Figure 5.—Computed radiation resistance.

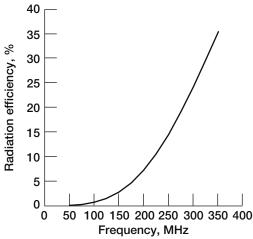


Figure 6.—Computed radiation efficiency.

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REPORT DOCUMENTATION PAGE

Form Approved OMB No. 0704-0188

Public reporting burden for this collection of information is estimated to average 1 hour per response, including the time for reviewing instructions, searching existing data sources, gathering and maintaining the data needed, and completing and reviewing the collection of information. Send comments regarding this burden estimate or any other aspect of this collection of information, including suggestions for reducing this burden, to Washington Headquarters Services, Directorate for Information Operations and Reports, 1215 Jefferson Davis Highway, Suite 1204, Arlington, VA 22202-4302, and to the Office of Management and Budget, Paperwork Reduction Project (0704-0188), Washington, DC 20503.

1. AGENCY USE ONLY (Leave blank)) 2. REPORT DATE	2. REPORT DATE 3. REPORT TYPE AND DATES COVERED	
	June 2004 Technical M		
4. TITLE AND SUBTITLE	TITLE AND SUBTITLE 5. FUN		
Printed Multi-Turn Loop A	ntenna for RF Bio-Telemetry		
6. AUTHOR(S)			WBS-22-251-30-15
Rainee N. Simons, David C	G. Hall, and Félix A. Miranda		
7. PERFORMING ORGANIZATION N	AME(S) AND ADDRESS(ES)		PERFORMING ORGANIZATION
National Aeronautics and Space Administration Labor H. Glanz Processes Contract Levels Field			E-14374
9. SPONSORING/MONITORING AGE	ENCY NAME(S) AND ADDRESS(ES)	10.	SPONSORING/MONITORING
National Agranguties and C	noon Administration		AGENCY REPORT NUMBER
National Aeronautics and Space Administration Washington, DC 20546–0001			NASA TM—2004-212982
11. SUPPLEMENTARY NOTES			
Meeting sponsored by the I Rainee N. Simons and Féli	nnas and Propagation Society In Institute of Electrical and Electron X A. Miranda, NASA Glenn Res Sponsible person, Rainee N. Sin	onics Engineers, Monterey, Cearch Center; and David G.	California, June 20–26, 2004. Hall, ZIN Technologies, Inc.,
12a. DISTRIBUTION/AVAILABILITY	STATEMENT	12b	. DISTRIBUTION CODE
Unclassified - Unlimited Subject Category: 33	Distrib	oution: Nonstandard	
Available electronically at http:/	//gltrs.grc.nasa.gov		
	m the NASA Center for AeroSpace In	formation, 301–621–0390.	
13. ABSTRACT (Maximum 200 word	ls)		
MEMS sensors at a design radiation resistance, skin ef The computed input reactar	frequency of 300 MHz is demon fect resistance, and radiation eff	nstrated. In addition, computations for the printed multi red values and shown to be i	telemetry from implantable bioted values of input reactance, -turn loop antenna are presented. n fair agreement. The computed
14. SUBJECT TERMS			15. NUMBER OF PAGES
Spiral inductors; Bio-MEMS; Bio-sensor system; Biomedical RF telemetry			16. PRICE CODE
17. SECURITY CLASSIFICATION OF REPORT	18. SECURITY CLASSIFICATION OF THIS PAGE	19. SECURITY CLASSIFICATION OF ABSTRACT	20. LIMITATION OF ABSTRACT
Unclassified	Unclassified	Unclassified	